

## Numerical Modeling of a Metamaterial Biosensor for Cancer Tissues Detection

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**Abstract:** In this paper, the numerical design and simulate a biosensor to detect tumors and cancerous tissues by using metamaterial structures in the microwave regime are presented. The presented structure consists of a microstrip transmission line and a split ring resonator (SRR) that form a bandpass filter and has a unique resonance frequency. Given that cancerous tissues have larger volumes of water than healthy tissues. As a result, they have a higher dielectric coefficient and conductivity which use for healthy tissues detection. By placing biological samples on SRR, its dielectric constant changes, therefore, the resonance frequency of the system changes. We can measure the types of biological tissues by measuring these changes. We used the Debye model to simulate the muscles. Also, the benefits of this biosensor are easy to use and operation, but they have lower sensitivity than terahertz biosensors. The minimum resolution for samples under test in this biosensor is 10 MHz.

**Keywords:** Biosensor, Microstrip Line, Split Ring Resonator, Cancerous Tissues, Debye Model.

### 1. INTRODUCTION

More recently, the metamaterials have been considered by several research groups due to their interesting optical properties including negative the dielectric constant ( $\epsilon$ ) and the magnetic permeability ( $\mu$ ) [1], as well as their application such as microsphere sensor [1], second harmonic generation [2], plasmonics sensor [3-7], biosensors [8-12], refractive and optical sensors [13-30], and etc [31-41]. One of the most critical features of this material is the negative refractive index as well as the guidance of electromagnetic waves in the desired direction [42-56]. It is worth mentioning that two dimensional material have been received much attention from research groups [57-58]. Considering the extremely high sensitivity of metamaterials to electromagnetic waves, they are also used as biological sensors. Conventional biological sensors

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(such as those works based on electromechanical transfer, fluorescence, nanomaterials and surface plasma resonance) often suffer from their very sophisticated equipment. In recent years, researchers have proposed the use of metamaterials for high sensitive to chemicals, biochemistry, and biological analytes. However, many of these structures suffer from their complicated fabrication and their cost.

In this paper, we design and simulate a low-cost and straightforward biosensor in the microwave ranges. The proposed sensor is made up of a macro strip line and a split ring resonator (SRR). The SRR can be considered as a simple LC circuit, which has a specific resonance frequency, which depends on the dimensions and the dielectric constant ( $\epsilon$ ). We also know that cancerous tissues and tumors have a higher content of water than healthy tissues. Hence, they have higher dielectric constant as well as conductivity. As a result, we can use these changes to detect these tissues from each other. By placing the tissues on the SRRs, the dielectric constant of the medium changes and the resonant frequency is then shifted. By measuring the rate of the shift, one can recognize the tissues and their types. Because the dielectric constant and the conductivity of biological tissues vary with frequency, we have used the Debye model to account for these effects.

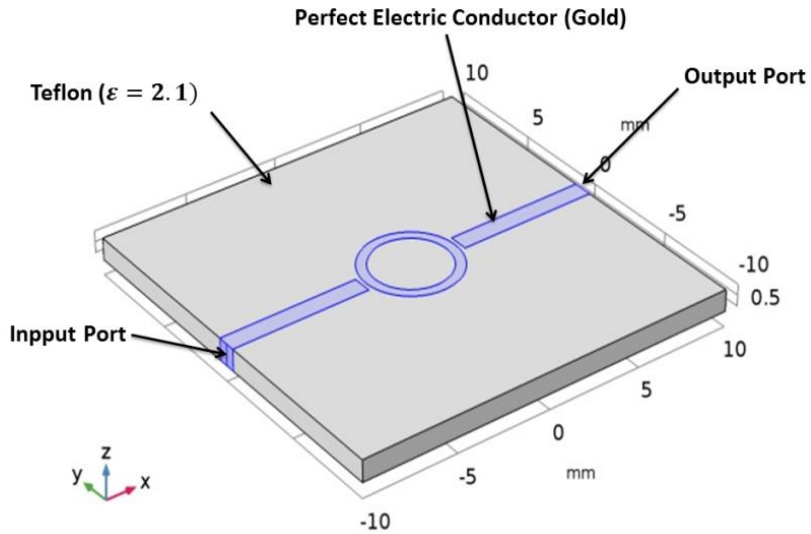
## 2. THE MODEL OF THE PROPOSED BIOSENSOR

The three-dimensional schematic of the proposed biosensor structure is shown in Fig. 1. As can be seen, this sensor is composed of a microstrip line and an SRR. Electric waves are emitted from the input port and measured at the output port. SR can be considered equivalent to a simple LC circuit.

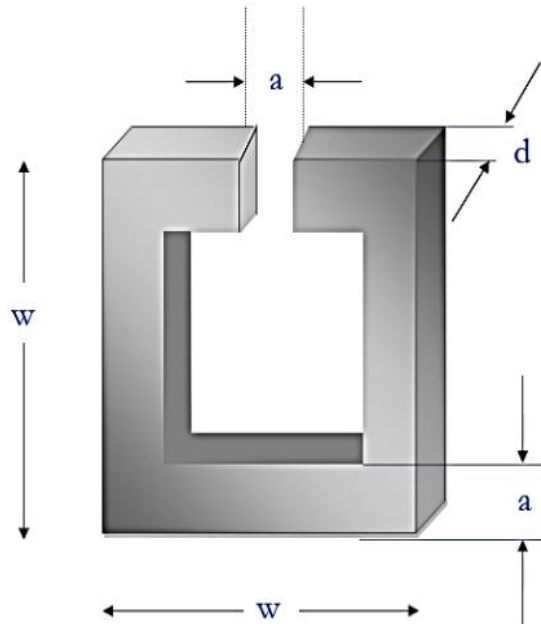
Fig. 2 shows an example of SRR whose resonant frequency is obtained by equation 1-2.

$$c = \epsilon_0 \epsilon_c \frac{d}{a}, L = \mu_0 \frac{w^2}{d_1} \quad (1)$$

$$\omega_{LC} = \frac{1}{\sqrt{LC}} = \frac{1}{w} \frac{c}{\sqrt{\epsilon_c}}, c = \frac{1}{\sqrt{\epsilon_0 \mu_0}} \quad (2)$$

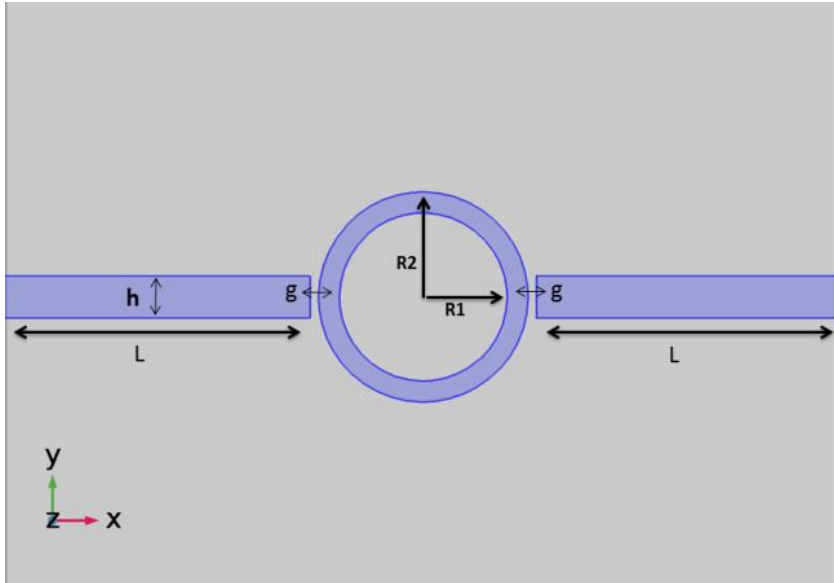


**Fig. 1** The overall shape of the proposed biosensor



**Fig. 2** An example of SRR

In the Fig. 3, the exact dimensions of sensor are considered that are  $L=7.3$  mm,  $h=1$  mm,  $g=0.2$  mm,  $R1=2$  mm, and  $R2=2.5$  mm.



**Fig. 3** Dimensions of the sensor

### 3. REQUIRED INFORMATION FOR SIMULATION

As mentioned in the earlier section, in this work, the Debye model is utilized; hence, in this section examines the essential information for simulation [59,60]. As we have mentioned, for the detection of tissues from each other, we use here the constant dielectric and conductivity changes in normal and malignant tissues. For modeling of biological tissues and simulate them, we use the Debye model whose relations are shown in Equations 3-5.

$$\varepsilon_{rc}(\omega) = \varepsilon_r(\omega) + i \frac{\sigma(\omega)}{\omega \varepsilon_0} \quad (3)$$

$$\varepsilon_r(\omega) = \varepsilon_\infty(\omega) + \frac{\varepsilon_s}{1 + (\omega\tau)^2} \quad (4)$$

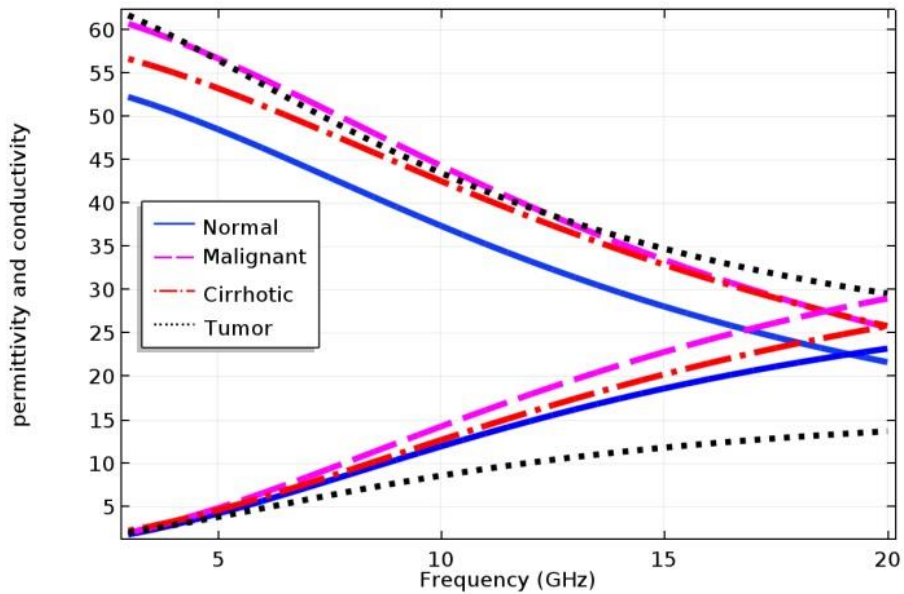
$$\sigma(\omega) = \omega^2 \tau \varepsilon_0 \frac{\varepsilon_s - \varepsilon_\infty}{1 + (\omega\tau)^2} + \sigma_s \quad (5)$$

The parameters extracted from the tissues of the body outside for healthy, cirrhotic, malignant, and tumor specimens are shown in the following table [61].

**Table I.** the parameters of *ex vivo*

Materials	$\tau$ [ps]	$\epsilon_{\infty}$	$\epsilon_s$	$\sigma_s$
Normal	11.55	5.32	49.55	0.25
Malignant	10.82	4.60	58.86	0.21
Cirrhotic	10.45	6.09	52.9	0.74
Tumor	15	18.8	46.8	0.803

The Fig. 4 illustrates the results of simulation of Debye model for relative permittivity (top charts) and effective conductivity (bottom charts) as a function of frequency for all the tissues including of normal, malignant, cirrhotic and tumor, respectively, in the frequency range between 1 to 20 GHz.



**Fig. 4.** Effective conductivity and relative permittivity VS frequency in the GHz regime

We used the reflection and transmission parameters to detect of tissues, which is obtained as  $T=|S_{21}|^2$  and  $R=|S_{11}|^2$ . The method used here for the process of simulating and solving differential equations is the finite element method (FEM) [62]. The FEM is an accurate numerical solution method based on meshed structures, and then equations and boundary conditions are solved in each mesh. This method is more precise than other methods and is well adapted to non-square structures. Also, the equations we want to solve using this method are the following equations:

$$\nabla \times \mu_r^{-1}(\nabla \times E) - k_0^2(\epsilon_r - \frac{j\sigma}{\omega\epsilon_0})E = 0 \quad (6)$$

$$E(x, y, z) = E(x, y)e^{ik_z z} \quad (7)$$

Here,  $E$  is the electric field,  $\mu_r$  and  $\omega$  are the relative permeability tensor and the angular frequency, respectively. The  $\sigma$  is the conductivity tensor,  $\epsilon_0$  is the permittivity of the vacuum,  $\epsilon_r$  is the relative permittivity tensor, and finally,  $k_0$  is the free space wave number.

#### 4. RESULTS AND DISCUSSION

As mentioned in section 1, the proposed sensor has a SRR structure [63], and acts as a band-pass filter, which has a resonant frequency. In Fig. 6, the reflection and transmission diagrams of the sensor are shown for a case in which there is no sample on it. In this case, the resonance frequency of the system is 15.3 GHz.

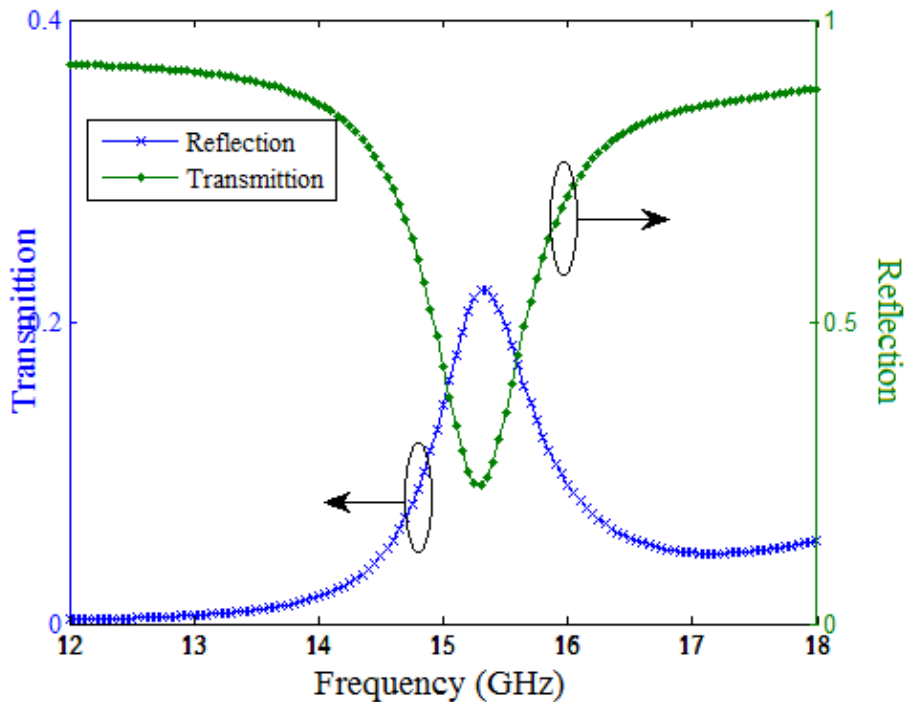
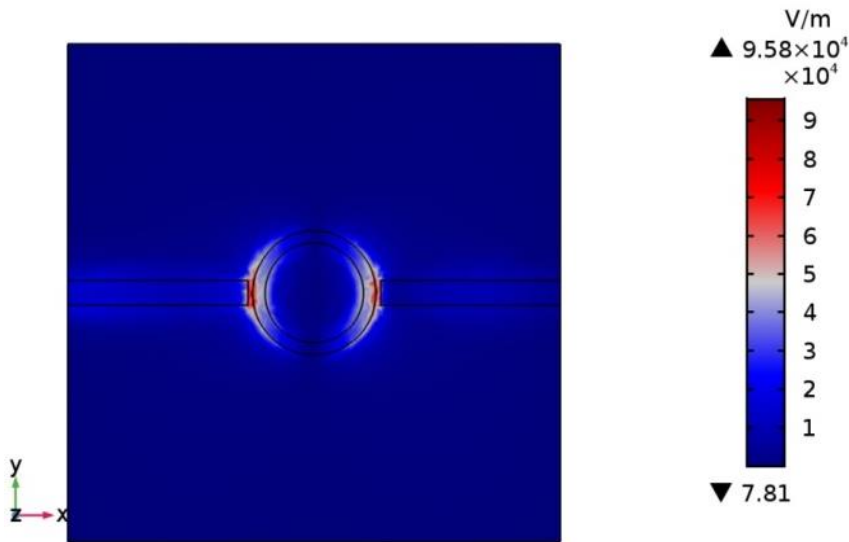


Fig. 6: The frequency response of the proposed biosensor

Also, in Fig. 7, we can see the distribution of the electric field at the resonance frequency. At this frequency, we will have the maximum transmission of electrical waves.

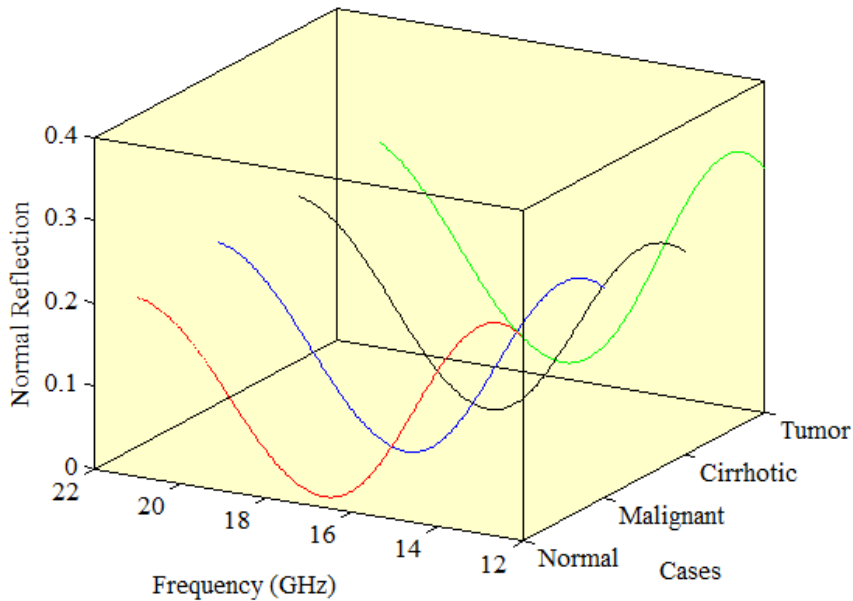


**Fig. 7:** Distribution of the electric field at a resonance frequency of 15.3 GHz

As mentioned in the previous section, if we put the samples, we show on the SRR, the dielectric constant of the medium is changed, and as a result, the resonant frequency of the system is shifted. In Fig. 8, these changes are shown for healthy, cirrhotic, malignant, and tumor tissues.

The changes in the resonance frequency of the system in various modes are respectively, 15.3 (no sample), 16.65 (standard sample), 16.6 (Cirrhotic), 16.59 (Malignant), and 16.7 (Tumor). As can be mentioned above, each of the tissues has a specific resonance frequency, which is due to their dielectric constant. According to the results, at least the resolution for the separation between the samples is about 10 MHz, which is related to the cirrhotic and malignant tissues. The maximum value is 110 MHz, which is related to malignant and tumor. In future the sensing behavior in our works is considered [64-66].

For future works, one-two dimensional can be considered [67-79].



**Fig. 8** The frequency response for all the tissues

## 5. CONCLUSION

In this paper, we simulated biosensor based on metamaterials for cancerous tissues detection in the microwave regime. Since biological tissues have certain dielectric constant and conductivity, we used this issue to identify them. In the absence of samples, the sensor has a specific resonance frequency, which, by placing the sample on it, will shift the frequency. The minimum and maximum resolution for the tested samples is 10 and 110 MHz. The advantages of this sensor include smooth operation and manufacturing.

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